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(54) **TREATMENT SYSTEM AND ACTUATION METHOD FOR TREATMENT SYSTEM**

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See application file for complete search history.

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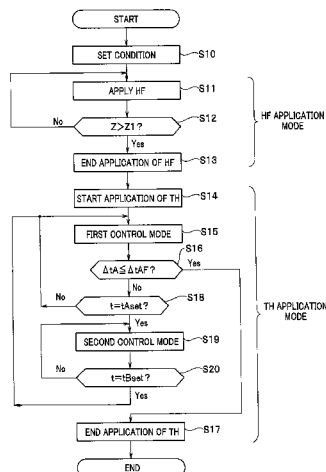
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ABSTRACT

A treatment system includes a power source for heat generation which outputs power for heat generation, a grasping member having a heating element which applies the power for heat generation as thermal energy to a grasped living tissue and is disposed at a grasping surface, and a control section which repeats a first control mode of performing control such that the heating element reaches a first temperature and a second control mode of performing control such that the heating element becomes lower than the first temperature, and controls the power source for heat generation according to a temperature change parameter based on change in temperature of the heating element in the first control mode or the second control mode so as to end application of the thermal energy.

16 Claims, 10 Drawing Sheets



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FIG. 1

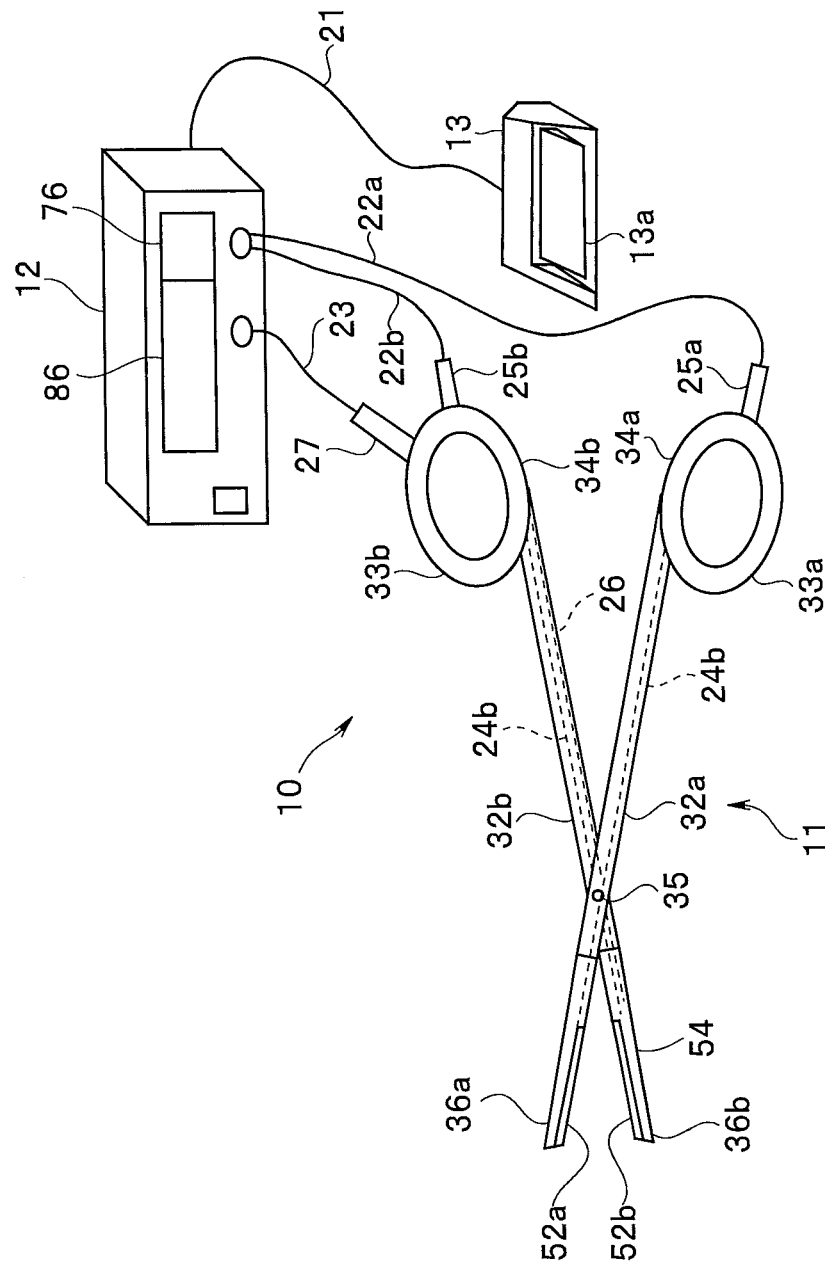


FIG. 2

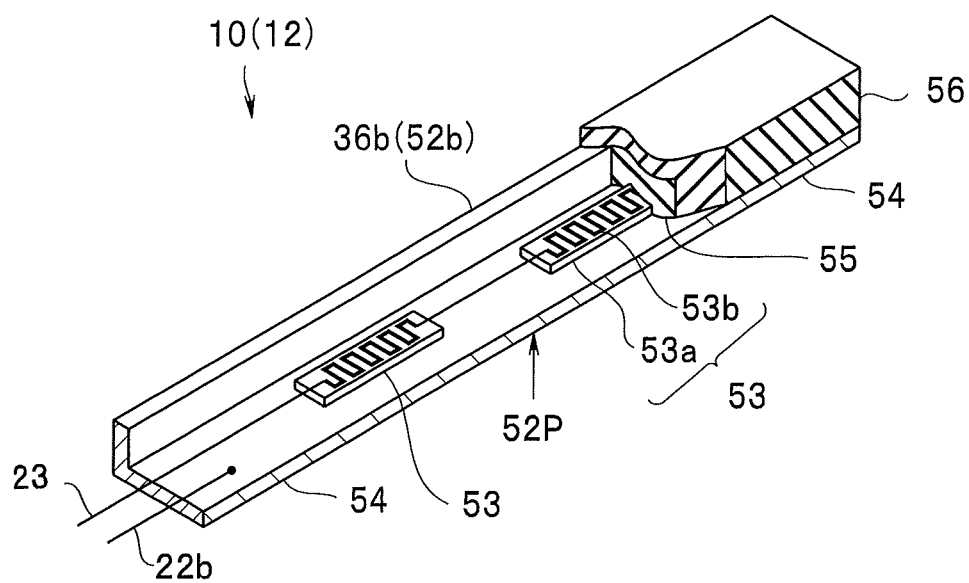


FIG. 3

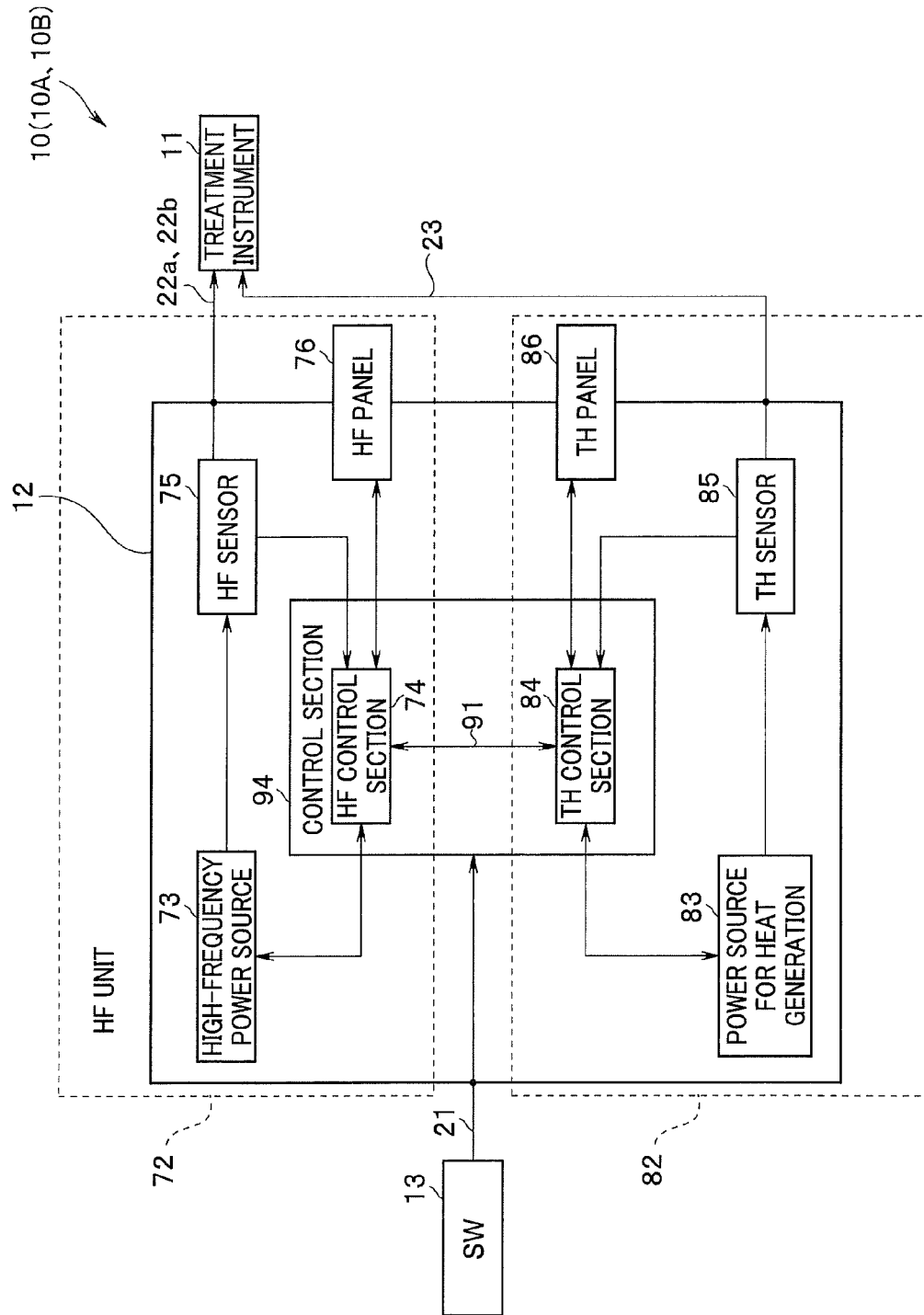


FIG. 4

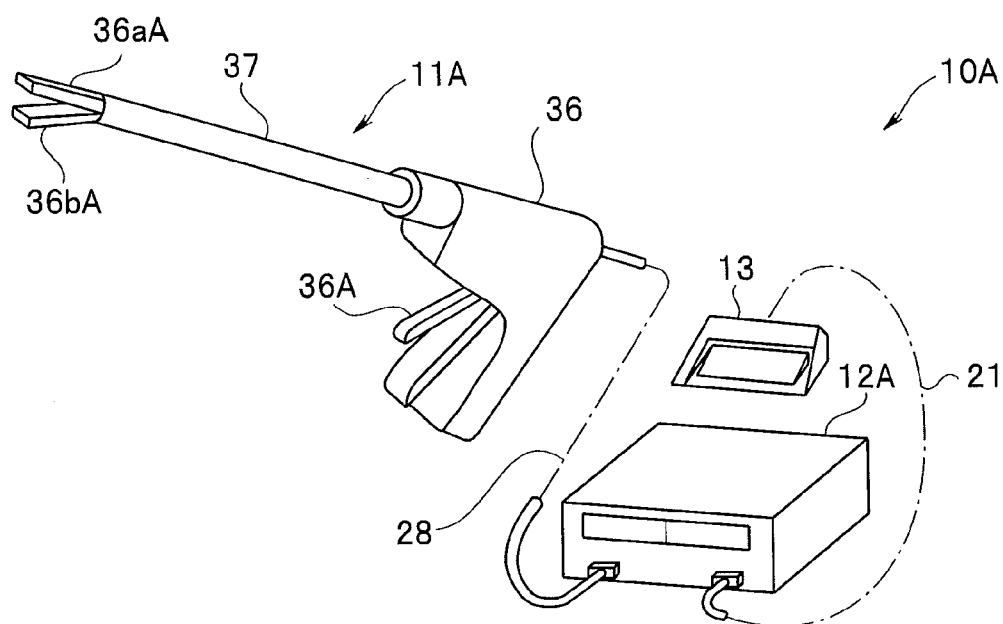


FIG. 5

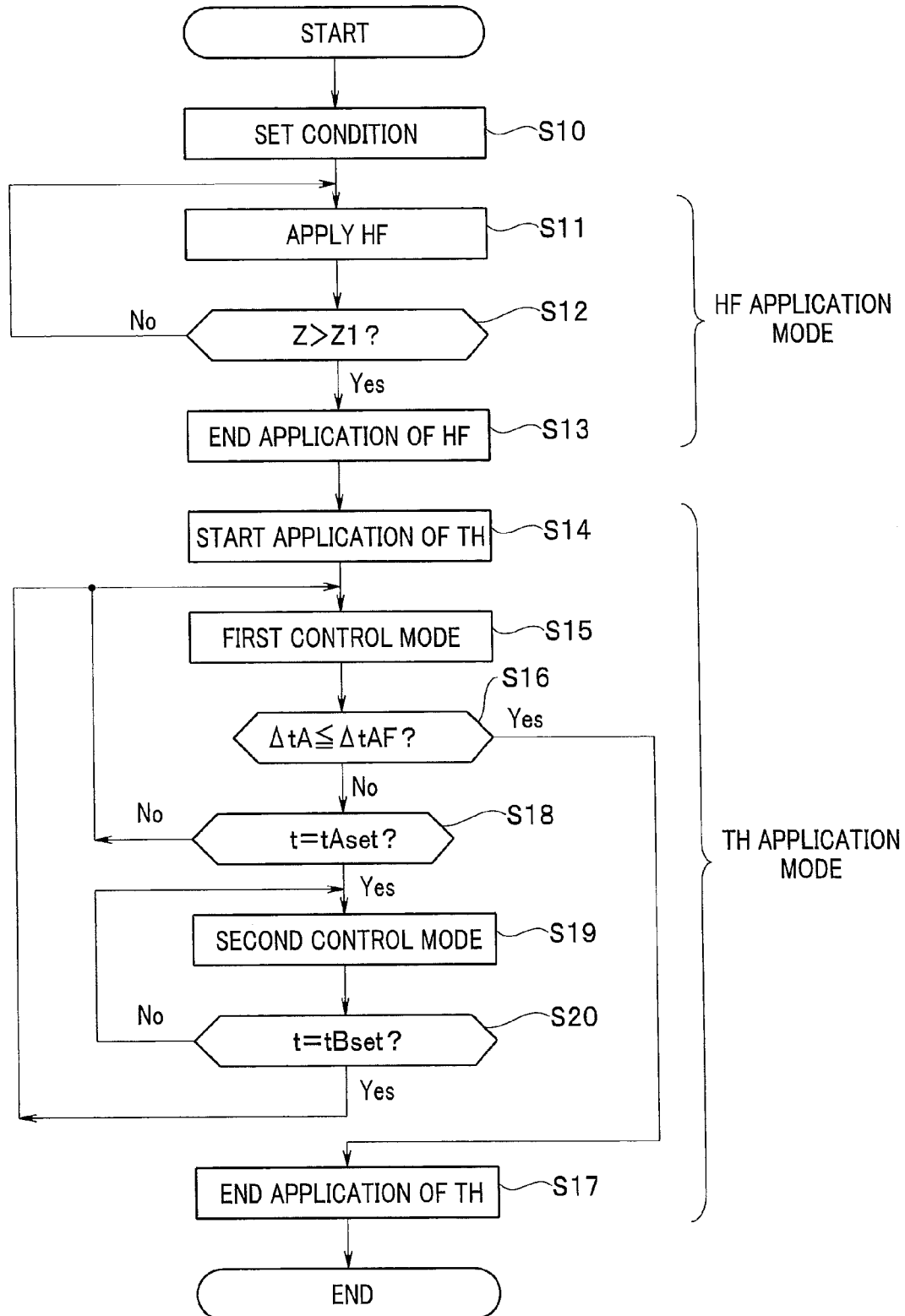


FIG. 6

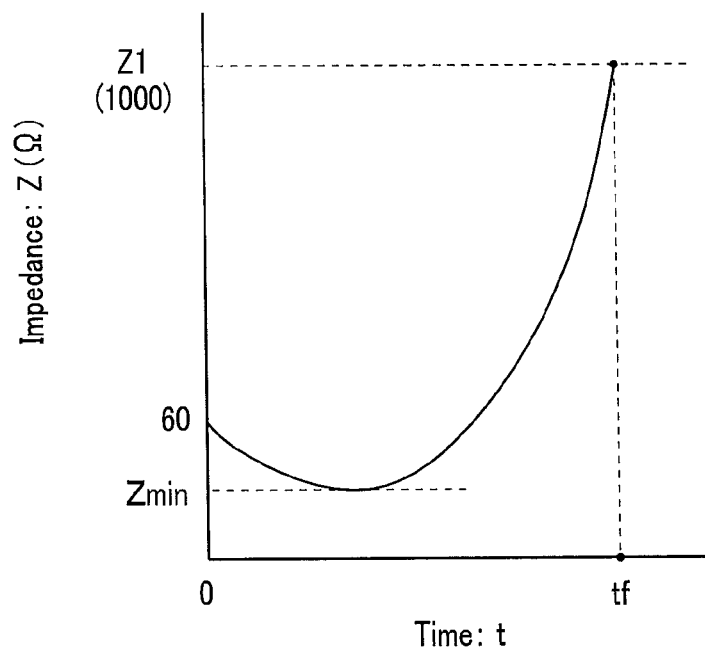


FIG. 7

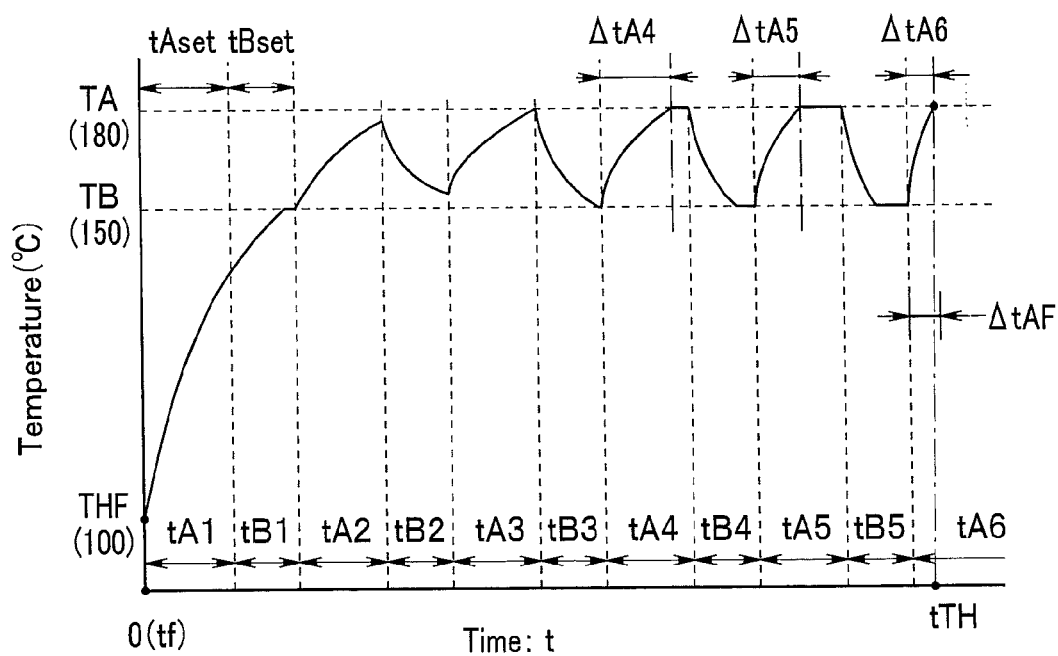


FIG. 8

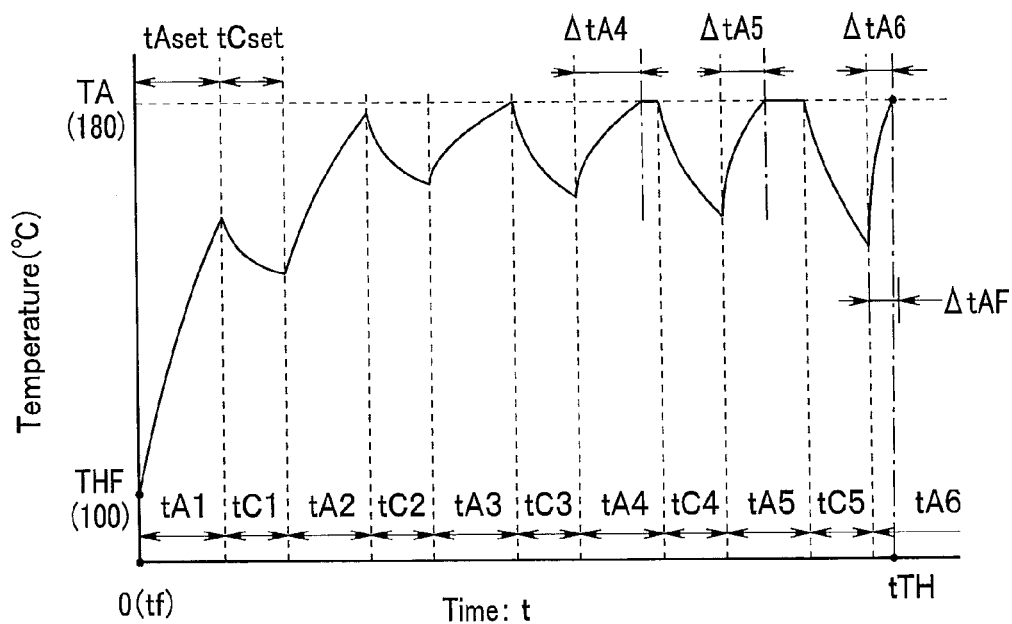


FIG. 9

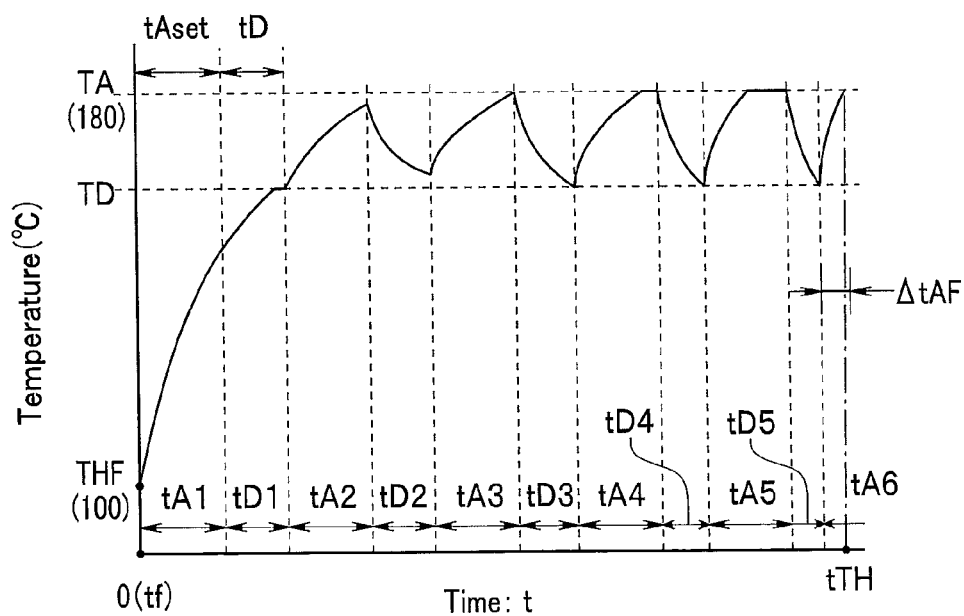


FIG. 10

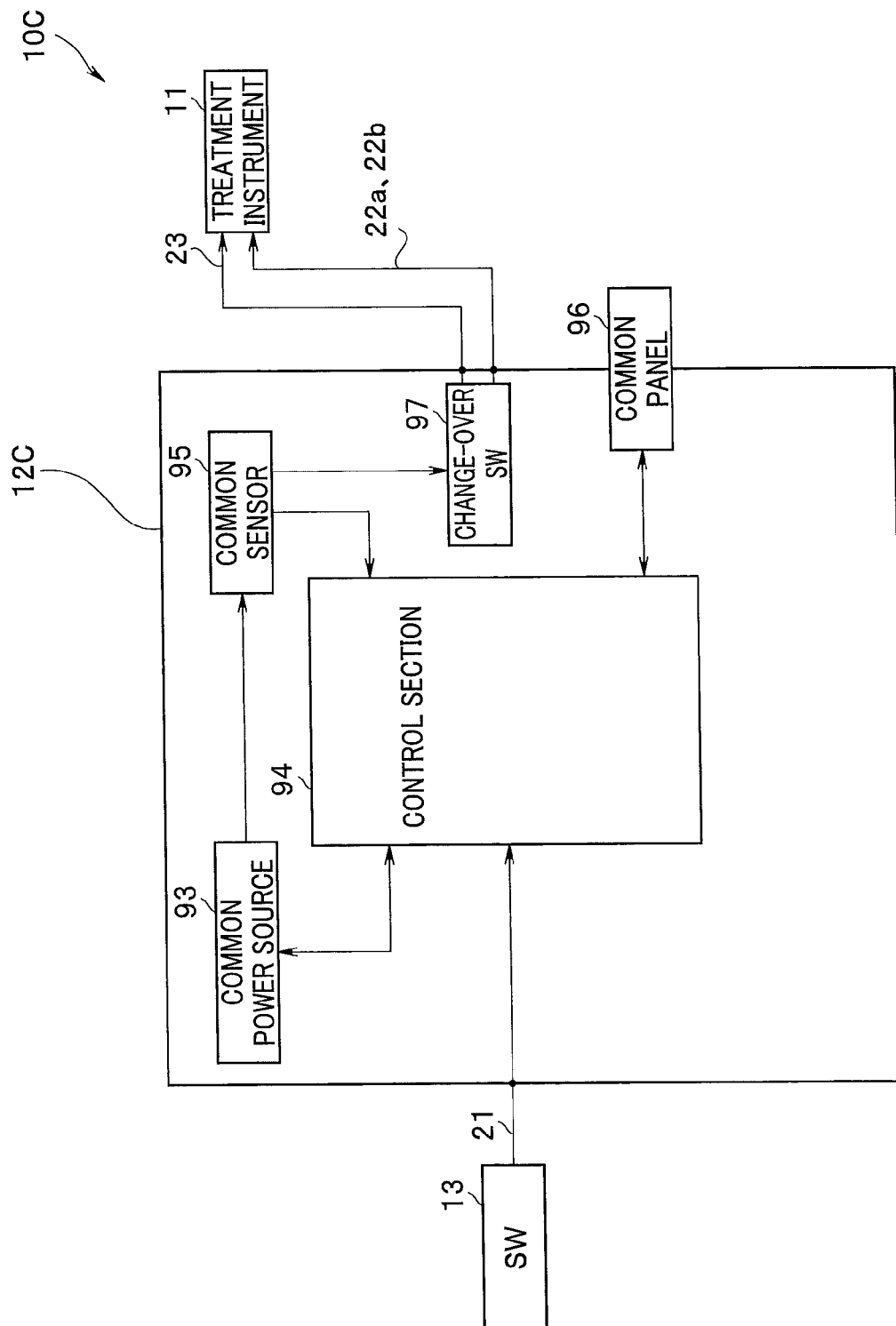


FIG. 11

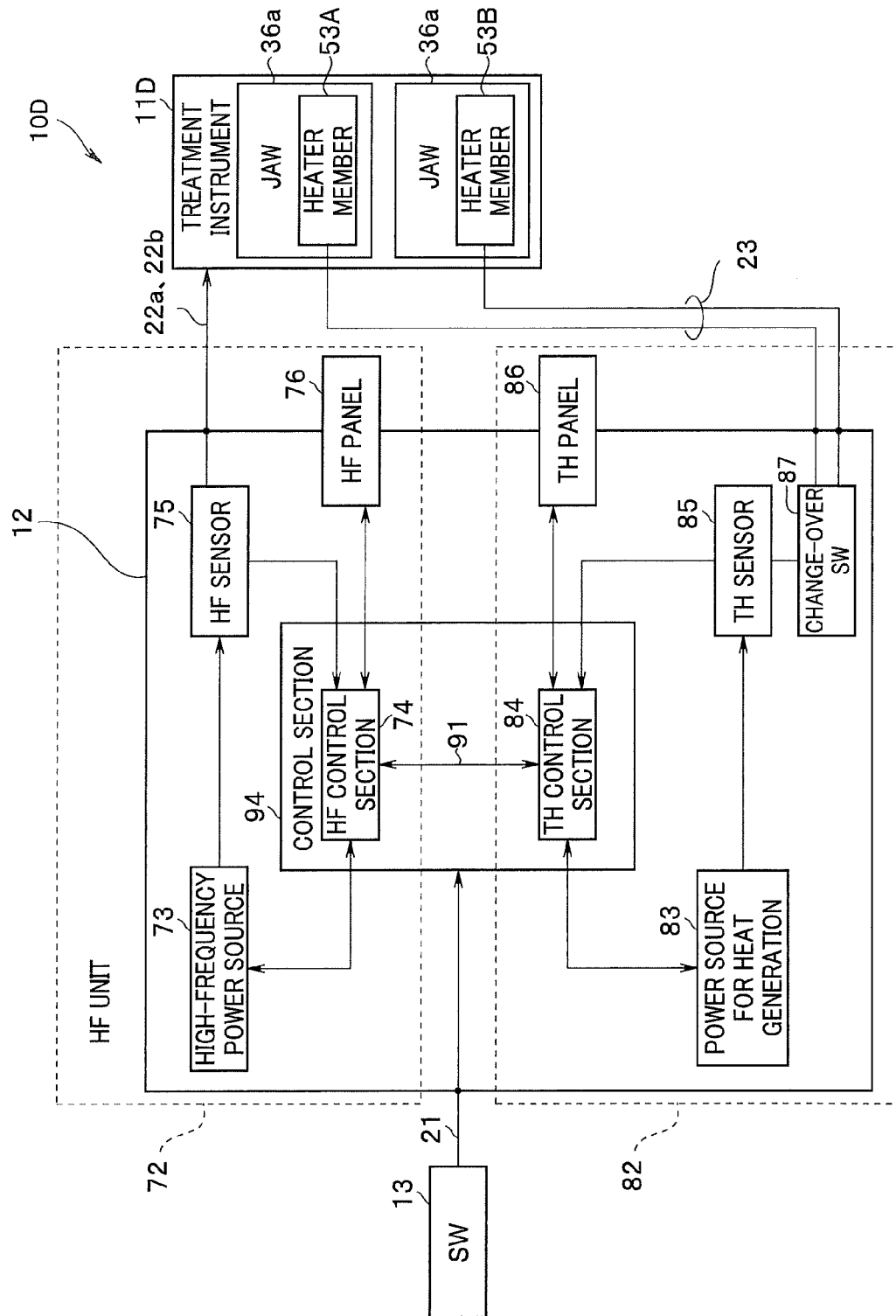
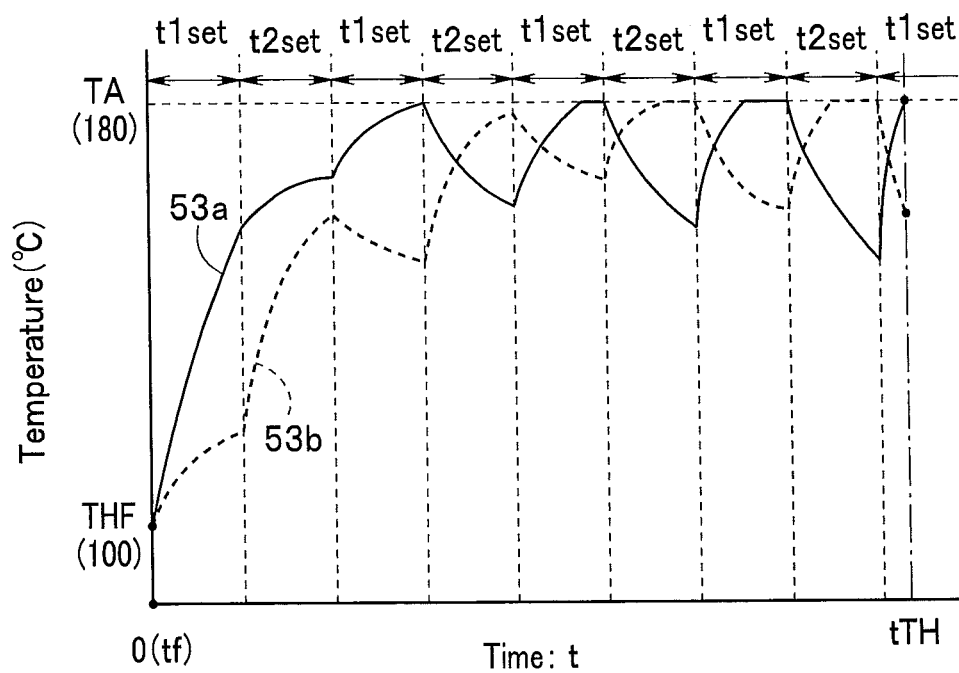


FIG. 12



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TREATMENT SYSTEM AND ACTUATION METHOD FOR TREATMENT SYSTEM

CROSS REFERENCE TO RELATED APPLICATION

This application is a continuation application of PCT/JP2012/079373 filed on Nov. 13, 2012 and claims benefit of U.S. Provisional Patent Application No. 61/569,336 filed in the U.S.A. on Dec. 12, 2011, the entire contents of which are incorporated herein by this reference.

BACKGROUND OF THE INVENTION

1. Field of the Invention

Embodiments of the present invention relate to a treatment system including one pair of grasping members which apply thermal energy to a grasped living tissue and an actuation method for the treatment system.

2. Description of the Related Art

U.S. Patent Application Publication No. 2009/076506 discloses a treatment system including one pair of grasping members which apply high-frequency power energy and thermal energy to a grasped living tissue, a high-frequency power source which outputs high-frequency power for applying high-frequency power energy, a power source for heat generation which outputs power for heat generation for applying thermal energy, and a control section which controls the high-frequency power source and the power source for heat generation for switching between application of high-frequency power energy and application of thermal energy.

U.S. Patent Application Publication No. 2009/0248002 discloses a treatment system which first applies high-frequency power energy to a living tissue and then starts application of thermal energy. High-frequency power energy acts to release intracellular components including polymer compounds typified by protein by destroying cell membranes in a living tissue and make the intracellular components uniformed with extracellular components typified by collagen. Such uniforming of a living tissue promotes joining of a living tissue through subsequent application of thermal energy.

For application of thermal energy, a process is known of raising temperature of a heating element to a predetermined temperature on the basis of a sensed temperature and then performing constant temperature control so as to hold the temperature at the predetermined temperature.

U.S. Patent Application Publication No. 2005/0222560 discloses a treatment instrument which performs temperature control by intermittently applying thermal energy, i.e., outputting power for heat generation.

SUMMARY OF THE INVENTION

A treatment system according to an embodiment includes a high-frequency power source which outputs high-frequency power, a power source for heat generation which outputs power for heat generation, one pair of grasping members having one pair of electric conductors which apply the high-frequency power as high-frequency power energy to a grasped living tissue and are disposed at respective grasping surfaces of the two grasping members and a heating element which applies the power for heat generation as thermal energy to the living tissue, is disposed at least one of the grasping members, and is made of a material having a positive temperature coefficient of resistance, and a control section which controls the high-frequency power source and the power source for heat generation after application of the high-frequency power energy ends so as to start application of the thermal energy, and repeats a first control mode of performing control such that the heating element reaches a first temperature and a second control mode of performing control such that the heating element becomes lower than the first temperature, and controls the power source for heat generation according to a temperature change parameter based on change in temperature of the heating element in the first control mode or the second control mode so as to end application of the thermal energy, after application of the thermal energy starts.

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An actuation method for a treatment system according to another embodiment includes a step of setting a treatment condition for the treatment system including one pair of grasping members which apply high-frequency power energy and thermal energy to a grasped living tissue, a high-frequency power source which outputs high-frequency power for applying the high-frequency power energy, and a power source for heat generation which outputs power for heat generation for applying the thermal energy, a step of controlling the high-frequency power source on the basis of the treatment condition and applying the high-frequency power energy to the living tissue, a step of acquiring a temperature change parameter, on the basis of change in temperature of the heating element in a first control mode of performing control such that the heating element reaches a first temperature or a second control mode of performing control such that the heating element becomes lower than the first temperature, during application of the thermal energy by repeating the first control mode and the second control mode on the basis of the treatment condition after application of the high-frequency power energy is ended on the basis of the treatment condition, and a step of ending application of the thermal energy according to the temperature change parameter.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is an external view of a treatment system according to a first embodiment;

FIG. 2 is a three-dimensional cross-sectional view for explaining a structure of a jaw in the treatment system according to the first embodiment;

FIG. 3 is a configuration diagram of the treatment system according to the first embodiment;

FIG. 4 is an external view of a treatment system according to a modification of the first embodiment;

FIG. 5 is a flowchart for explaining a flow of processing of the treatment system according to the first embodiment;

FIG. 6 is a graph showing change in impedance in high-frequency power application mode;

FIG. 7 is a graph showing change in temperature in power-for-heat-generation application mode in the treatment system according to the first embodiment;

FIG. 8 is a graph showing change in temperature in power-for-heat-generation application mode in a treatment system according to a second embodiment;

FIG. 9 is a graph showing change in temperature in power-for-heat-generation application mode in a treatment system according to a third embodiment;

FIG. 10 is a configuration diagram of a treatment system according to a fourth embodiment;

FIG. 11 is a configuration diagram of a treatment system according to a fifth embodiment; and

FIG. 12 is a graph showing change in temperature in power-for-heat-generation application mode in the treatment system according to the fifth embodiment.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

First Embodiment

Configuration of Treatment System

A treatment system **10** according to a first embodiment will first be described.

As shown in FIG. 1, the treatment system **10** includes a treatment instrument **11**, a power supply portion **12**, and a foot switch **13**. The treatment system **10** switches between high-frequency power energy and thermal energy and applies, using the power supply portion **12**, the energy to a living tissue grasped by jaws **36a** and **36b** which are one pair of grasping members of the treatment instrument **11**. Note that high-frequency power and power for heat generation may hereinafter be abbreviated as “HF” and “TH,” respectively. For example, high-frequency power energy is referred to as HF energy.

The treatment instrument **11** is connected to the power supply portion **12** by HF lines **22a** and **22b** and a TH line **23**. Note that although the HF lines **22a** and **22b**, the TH line **23**, and the like each have two pieces of wiring, the two pieces of wiring are expressed as one line. The foot switch **13** is connected to the power supply portion **12** by a switch line **21**.

The treatment instrument **11** has one pair of scissors constituent members **32a** and **32b**, one pair of handle portions **34a** and **34b**, and the one pair of jaws **36a** and **36b**. The handle portions **34a** and **34b** are provided at proximal end portions of the scissors constituent members **32a** and **32b**. The handle portions **34a** and **34b** are operated while being held in a hand by a surgeon. The jaws **36a** and **36b** are provided at distal end portions of the scissors constituent members **32a** and **32b** to grasp a living tissue to be treated.

The scissors constituent members **32a** and **32b** are placed one on the other so as to substantially intersect each other between distal ends and proximal ends of the scissors constituent members **32a** and **32b**. A fulcrum pin **35** which pivotably couples the scissors constituent members **32a** and **32b** is provided at an intersection portion of the scissors constituent members **32a** and **32b**.

The handle portions **34a** and **34b** are provided with rings **33a** and **33b** on which a surgeon puts his or her fingers. When the surgeon puts a thumb and a middle finger through the rings **33a** and **33b**, respectively, and opens and closes the rings **33a** and **33b**, the jaws **36a** and **36b** open and close in tandem with the motion.

Respective energy release elements which apply energy to a grasped living tissue are disposed at the jaws **36a** and **36b**. That is, an electrode **52a** as the energy release element which has a grasping surface and is made of an electric conductor is disposed at the jaw **36a**. An electrode **52b** as the energy release element which has a grasping surface and is made of an electric conductor and a heater member **53** as a heating element are disposed at the jaw **36b**. The heater member **53** is embedded in the jaw **36b** while the heater member **53** is disposed on a reverse surface of the electrode **52b** that is made of a high thermal conductor.

That is, as shown in FIG. 2, in the jaw **36b** of the treatment instrument **11**, the heater member **53** is joined to a surface reverse to a grasping surface **52P** of a base **54** which is made of copper. The heater member **53** is covered with a sealing member **55** and a cover member **56**. Note that FIG. 2 shows a portion of the jaw **36b** and that three or more heater members **53** may be joined to each jaw **36b**.

In the heater member **53**, a thin-film resistor or a thick-film resistor is disposed as a heating pattern **53b** on a substrate **53a** of, e.g., alumina or aluminum nitride. The thin-film resistor is made of, e.g., an electrically conductive thin film which is formed by a thin film formation method, such as PVD (physical vapor deposition) or CVD (chemical vapor deposition), or foil of an electrically conductive metal, such as SUS. The thick-film resistor is formed by a thick film formation method, such as screen printing. The heating pattern **53b** is formed of a refractory metal material, such as molybdenum, which exhibits a positive temperature coefficient of resistance indicating that electric resistance increases directly with temperature.

Note that the heater member **53** may also be disposed at the jaw **36a** of the treatment instrument **11**. That is, a heating element only needs to be disposed at least one grasping member.

HF lines **24a** and **24b** for supplying HF to the electrodes **52a** and **52b** are disposed inside the scissors constituent members **32a** and **32b**, respectively. The HF lines **24a** and **24b** extend from the jaws **36a** and **36b** to the handle portions **34a** and **34b**, respectively. HF terminals **25a** and **25b** are provided at the rings **33a** and **33b**, respectively. The HF terminals **25a** and **25b** are connected to the HF lines **24a** and **24b**, respectively. For the reason, when HF is supplied to the electrodes **52a** and **52b** while a living tissue is grasped by the jaws **36a** and **36b**, HF is passed through the living tissue between the electrodes **52a** and **52b**. In other words, HF energy is applied to the living tissue.

A TH line **26** for supplying TH to the heater member **53** is disposed inside the scissors constituent member **32b**. The TH line **26** extends from the jaw **36b** to the handle portion **34b**. A TH terminal **27** which is connected to the TH line **26** is provided at the ring **33b**. For the reason, when TH is supplied to the heater member **53** through the TH line **26**, the heater member **53** generates heat. That is, the TH is converted into thermal energy by the heater member **53**, the thermal energy is transferred to the electrode **52b**, and the thermal energy is applied to a living tissue in contact with the grasping surface of the electrode **52b**.

As described above, when HF is passed between the electrodes **52a** and **52b**, the treatment instrument **11** applies HF energy to a living tissue grasped between the jaws **36a** and **36b**. When TH is passed through the heater member **53** in the treatment instrument **11**, the TH is converted into the thermal energy. The treatment instrument **11** applies the thermal energy to the living tissue.

The foot switch **13** has a pedal **13a**. While the pedal **13a** is pressed, the power supply portion **12** outputs HF or TH on the basis of a setting state (a state in which an output value, output timing, and the like are controlled). When the press of the pedal **13a** is canceled, the power supply portion **12** forcibly stops outputting the power.

As shown in FIG. 3, the power supply portion **12** is composed of an HF unit **72** and a TH unit **82**. The HF unit **72** has a high-frequency power source **73** which outputs HF, an HF control section **74** which controls the high-frequency power source **73** and is made up of a semiconductor circuit, such as a CPU, and the like, an HF sensor **75** which is a high-frequency power measuring section which measures voltage and current of HF outputted by the high-frequency power source **73**, and an operation panel **76**.

The TH unit **82** has a power source **83** for heat generation which outputs TH, a TH control section **84** which controls the power source **83** for heat generation and is made up of a semiconductor circuit, such as a CPU, and the like, a TH sensor **85** which is a heat generation power measuring section

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that measures voltage and current of TH outputted by the power source **83** for heat generation, and an operation panel **86**.

The HF control section **74** and the TH control section **84** are connected by a communication line **91** which can transmit a signal in both directions to constitute a control section **94**. That is, the control section **94** controls the high-frequency power source **73** and the power source **83** for heat generation. The operation panels **76** and **86** each have a setting function portion, with which a surgeon sets a treatment condition, and a display function of displaying a treatment status.

The HF sensor **75** is connected to the treatment instrument **11** via the HF lines **22a** and **22b**. The high-frequency power source **73** and the HF sensor **75** are connected to the HF control section **74**. The HF control section **74** is further connected to the operation panel **76**. The HF control section **74** calculates HF information, such as power and impedance, on the basis of information from the HF sensor **75**, sends a control signal to the high-frequency power source **73**, and sends information to be displayed to the operation panel **76**. HF outputted by the high-frequency power source **73** that is controlled by the HF control section **74** is transmitted to the electrodes **52a** and **52b** of the treatment instrument **11**.

The TH control section **84** calculates temperature of the heater member **53** as TH information on the basis of information from the TH sensor **85**, in addition to power, a resistance value, and the like. That is, since the heating pattern of the heater member **53** is made of a material having a positive temperature coefficient of resistance, as already described, the TH control section **84** can calculate the temperature of the heater member **53** from a TH resistance value which is calculated from voltage and current of TH. The TH control section **84** sends a control signal to the power source **83** for heat generation on the basis of the TH information. TH outputted by the power source **83** for heat generation that is controlled by the TH control section **84** is transmitted to the heater member **53** of the treatment instrument **11**.

Note that the HF control section **74** also sends a control signal to the TH control section **84** at the end of application of HF such that the TH control section **84** starts outputting TH.

As described above, the treatment instrument **11** has a function of a bipolar-type high-frequency treatment instrument and a function of a treatment instrument for heat generation.

Note that the treatment instrument of the treatment system according to the embodiment may be a so-called linear-type treatment instrument. For example, a treatment system **10A** according to a modification shown in FIG. **4** includes a linear-type treatment instrument **11A**, a power supply portion **12A**, and the foot switch **13**.

The treatment instrument **11A** has a handle **36**, a shaft **37**, and one pair of jaws **36aA** and **36bA** which are grasping members that grasp a living tissue. Structures of the jaws **36aA** and **36bA** are identical to the structures of the jaws **36a** and **36b**.

The handle **36** has a shape which is easy for a surgeon to grip, such as a substantially L-shape. The handle **36** has an open/close knob **36A**. The open/close knob **36A** is designed such that the jaws **36a** and **36b** grasp a living tissue when a surgeon presses and operates the open/close knob **36A**. HV electrodes (not shown) and heater members (not shown) of the jaws **36aA** and **36bA** are connected to the power supply portion **12A** via a piece **28** of wiring. That is, the piece **28** of wiring is made up of the HF lines **22a** and **22b** and the TH line **23**. A basic configuration and a function of the power supply portion **12A** are identical to the basic configuration and the function of the power supply portion **12**.

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That is, any of treatment instruments having various structures can be used as long as the treatment instrument can apply high-frequency power energy and thermal energy to a grasped living tissue.

Motion of Treatment System

An actuation method for the treatment system **10** will be described.

The treatment system **10** first applies HF energy to a grasped living tissue and applies thermal energy after the application of HF energy ends. In other words, the control section **94** controls the high-frequency power source **73** and the power source **83** for heat generation to start applying thermal energy after application of high-frequency power energy ends.

Application of thermal energy to a living tissue for more than a proper time period not only brings about no improvement in effectiveness but also has adverse effects, such as adherence of the living tissue to a treatment surface. For the reason, application of thermal energy needs to be ended at a proper time. Proper application end times, however, vary according to the type, size, and the like of a living tissue being treated. A user thus needs to monitor a treatment status and end application of thermal energy on the basis of experience and the like.

When a process of destroying cell membranes in a living tissue is completed through application of HF energy, switching from HF energy application mode to thermal energy application mode is performed. In thermal energy application mode, moisture is removed by further raising temperature of the living tissue, and a process of joining the living tissue is performed through hydrogen bonding.

Treatment is completed by stopping application of thermal energy when the joining process is appropriately ended. Since the control section **94** (the TH control section **84**) automatically ends application of thermal energy in a proper time period on the basis of change in temperature, the treatment system **10** has good operability.

A motion of the treatment system **10** will be described below in detail with reference to a flowchart shown in FIG. **5**.

Step S10

A surgeon inputs and sets treatment conditions to the control section **94** by using the operation panels **76** and **86**. Examples of the treatment conditions include setting power Pset (W) for HF energy application mode, a setting temperature Tset (° C.) for thermal energy application mode, and a threshold value Z1 (Ω) for an HF impedance Z for determining when to end HF energy application mode. Note that the treatment conditions will be described in detail later.

Step S11

The surgeon puts his or her fingers on the rings **33a** and **33b** of the handle portions **34a** and **34b** of the treatment instrument **11**, operates the treatment instrument **11**, and grasps a living tissue to be treated with the jaws **36a** and **36b**.

When the surgeon presses the pedal **13a** of the foot switch **13** with a foot, application of HV energy to the living tissue between the electrodes **52a** and **52b** of the jaws **36a** and **36b** of the treatment instrument **11** starts. Note that the pedal **13a** remains pressed during treatment. When the surgeon takes the foot off the pedal **13a**, the power supply portion **12** forcibly stops outputting the energy.

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HV outputted by the high-frequency power source **73** is controlled by constant power control to a predetermined setting power P_{set} (e.g., about 20 W to 150 W).

In HF energy application mode, Joule heat is generated to heat the living tissue itself. Dielectric breakdown, electric discharge, and the like arising from HF action destroy cell membranes in the living tissue. With the destruction of the cell membranes, released materials from the cell membranes are uniformed with extracellular components typified by collagen.

In HF energy application mode, the impedance Z for HF, i.e., the impedance Z in the grasped living tissue is calculated on the basis of HF information from the HF sensor **75**. As shown in FIG. 6, the impedance Z is, for example, about 60Ω at the start of the HF energy application, decrease after the start to exhibit a minimum value Z_{min} , and increase after the exhibition.

Step S12

Since application of HF energy advances drying of the living tissue, the impedance Z for HF rises. Completion of the process of destroying cell membranes in the grasped living tissue is sensed on the basis of the impedance Z . That is, since when the destruction process is completed, substances in cell membranes are released no longer, rise in the impedance Z accelerates. Additionally, when the impedance Z is high, appropriate HF energy application is difficult.

For the reason, the control section **94** (the HF control section **74**) determines, on the basis of a predetermined threshold value $Z1$, whether to end HF energy application mode.

The threshold value $Z1$ is, for example, about 10Ω to 1500Ω . Note that the surgeon need not set the threshold value $Z1$ if the threshold value $Z1$ is incorporated in advance in a program of the control section **94** (the HF control section **74**). Alternatively, whether to end HF energy application mode may be determined by another method.

The HF control section **74** determines whether the impedance Z has exceeded the threshold value $Z1$ (e.g., 1000Ω). If the HF control section **74** determines that a value of the impedance Z is less than the threshold value $Z1$ (NO in **S12**), the HF control section **74** continues applying HF energy.

Step S13

On the other hand, if the HF control section **74** determines that the impedance Z has exceeded the threshold value $Z1$ (YES in **S12**), the HF control section **74** controls the high-frequency power source **73** so as to stop outputting HF.

Step S14

If the HF control section **74** determines that the impedance Z has become not less than the threshold value $Z1$, a signal is transmitted from the HF control section **74** of the HF unit **72** to the TH control section **84** of the TH unit **82** via the communication line **91**. Switching from HF energy application mode to TH energy application mode is performed.

In TH energy application mode, by further raising a temperature T of the heater member **53**, proteins in the living tissue are integrally denatured, and removal of moisture that is a hindrance to hydrogen bonding between proteins is performed.

In the treatment system **10**, the TH control section **84** repeats, in TH energy application mode, a first control mode of performing constant temperature control (feedback con-

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trol) such that the temperature of the heater member **53** reaches a first temperature T_A and a second control mode of performing constant temperature control (feedback control) such that the heater member **53** reaches a second temperature T_B which is lower than the first temperature T_A .

Step S15

Change in the temperature of the heater member **53** in a case where the first temperature T_A and the second temperature T_B are 180°C . and 150°C ., respectively, in TH energy application mode is shown in FIG. 7.

A temperature T_{HF} of the heater member **53** when TH energy application mode starts, i.e., HF energy application mode ends (tf) is, for example, 100°C .

During the first control mode ($tA1$ to $tA6$), the TH control section **84** controls the power source **83** for heat generation such that the temperature of the heater member **53** reaches the first temperature T_A .

Step S16

The TH control section **84** determines whether a time period Δt_A for the temperature of the heater member **53** to reach the first temperature T_A is not more than a predetermined threshold time period (Δt_{AF}).

Step S17

If the time period Δt_A is not more than the predetermined threshold time period (Δt_{AF}) (YES in **S16**), i.e., at a time t_{TH} , the control section **94** controls the power source **83** for heat generation so as to end application of thermal energy.

Step S18

If the time period Δt_A exceeds the predetermined threshold time period (Δt_{AF}) (NO in **S15**), the control section **94** continues application of thermal energy in a first control mode until a first control mode setting time period (t_{Aset}) is reached (NO in **S18**). That is, the processes from step **S16** are repeated.

Step S19

When the first control mode setting time period (t_{Aset}) has elapsed (YES in **S18**), the TH control section **84** changes control mode to a second control mode ($tB1$ to $tB5$) of controlling the power source **83** for heat generation such that the temperature of the heater member **53** reaches the second temperature T_B .

Step S20

The control section **94** continues application of thermal energy in the second control mode until a second control mode setting time period (t_{Bset}) is reached (NO in **S20**). That is, the processes from step **S19** are repeated.

On the other hand, when the second control mode setting time period (t_{Bset}) has elapsed (YES in **S20**), the processes from step **S15**, i.e., the processes in the first control mode are performed again.

As described above, in the treatment system **10**, the control section **94** controls the power source **83** for heat generation so as to end application of thermal energy by determining in step **S16** whether the time period Δt_A for the temperature T of the

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heater member **53** to reach the first temperature TA is not more than the predetermined threshold time period (ΔtAF).

Referring to FIG. 7, in the first control mode (tA1) for a first time, the temperature T of the heater member **53** rises from the temperature THF (100° C.) at the HF energy application mode end time (t=0 (tf)) but does not arrive at the first temperature TA. In the subsequent second control mode (tB1) for a first time, the temperature T rises further and arrives at the second temperature TB.

In the first control mode (tA2), the temperature T rises from the second temperature TB and does not arrive at the first temperature TA. In the second control mode (tB2), since the temperature T in an initial stage is higher than the second temperature TB, the temperature T decreases. In the first control mode (tA3), the temperature T rises and arrives at the first temperature TA. After tA3, the temperature T decreases in the second control mode (tB3, tB4, and tB5) while the temperature T rises in the first control mode (tA4, tA5, and tA6).

As shown in FIG. 7, in the first control mode, the time period (ΔTA) for the temperature T to rise to arrive at the first temperature TA decreases in the order: $\Delta tA4$, $\Delta tA5$, and $\Delta tA6$. This is because moisture in the grasped living tissue decreases by application of thermal energy, and thermal capacity becomes low. That is, a change in status of the living tissue due to proceeding of the treatment can be determined by the time period (ΔTA) to arrive at the first temperature TA.

The control section **94** controls the power source **83** for heat generation so as to end application of thermal energy by using the time period (ΔTA) to arrive at the first temperature TA as a temperature change parameter based on change in the temperature of the heater member **53** in the first control mode.

That is, the treatment system **10** repeats a first control mode of performing control such that the heater member **53** reaches the first temperature TA and a second control mode of performing control such that the heater member **53** becomes lower than the first temperature TA and ends application of thermal energy on the basis of the temperature change parameter based on change in the temperature of the heater member **53** in the first control mode.

The treatment system **10** can perform proper treatment by ending application of thermal energy when the time period (ΔTA) to arrive at the first temperature TA becomes not more than the predetermined threshold time period (ΔtAF), even if the type, size, initial moisture content, and the like of a living tissue being processed are different.

That is, the treatment system **10** and an actuation method for the treatment system **10** are capable of removing moisture from a living tissue and joining the living tissue through hydrogen bonding and then automatically completing treatment in an appropriate manner without applying excessive heat to the living tissue, even if the type and the like of the grasped living tissue are different. The treatment system **10** and the actuation method for the treatment system **10** are thus good in operability.

Note that the first temperature TA is set to a treatment temperature (e.g., 120° C. to 300° C.) and that the second temperature TB is set to, for example, 120° C. to 300° C. lower by 10° C. to 100° C. than the first temperature TA. If the second temperature TB is within the above-described range, detection accuracy for the time period (ΔTA) to arrive at the first temperature TA is high, and the treatment can be properly completed. The second control mode setting time period (tB-set) is preferably shorter than the first control mode setting time period (tA-set) in order to complete the process in a short time period.

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Note that a rate ($\Delta T/\Delta t$) of change in temperature in the first control mode may be used as the temperature change parameter instead of the time period (ΔTA) to arrive at the first temperature TA in the first control mode.

Alternatively, a time period to arrive at the second temperature TB in the second control mode or a rate ($\Delta T/\Delta t$) of change in temperature in the second control mode may be used as the temperature change parameter.

Alternatively, the plurality of parameters described may be used in combination as the temperature change parameter. That is, as the temperature change parameter, at least one of a time period to arrive at a predetermined temperature and a rate of change in temperature can be used.

Second Embodiment

A treatment system **10A** according to a second embodiment will be described. Since the treatment system **10A** is similar to the treatment system **10**, constituent elements having identical functions are denoted by identical reference numerals, and a description of the constituent elements will be omitted.

As shown in FIG. 8, in the treatment system **10A**, a TH control section **84** repeats, in TH energy application mode, a first control mode of performing control such that temperature of a heater member **53** reaches a first temperature TA and a second control mode of controlling a power source **83** for heat generation so as to suspend outputting power (TH) for heat generation such that the heater member **53** becomes lower than the first temperature TA.

A temperature T of the heater member **53** rises in the first control mode (tA1 to tA6) and decreases in the second control mode (tC1 to tC5).

The treatment system **10A** uses, as a temperature change parameter based on change in the temperature of the heater member **53**, a time period (ΔTA) to arrive at the first temperature TA or a rate ($\Delta T/\Delta t$) of rise in temperature in the first control mode or a time period (ΔTX) to arrive at a predetermined temperature TX or a rate ($\Delta T/\Delta t$) of decrease in temperature in the second control mode, like the treatment system **10**. With the use, the treatment system **10A** controls the power source **83** for heat generation so as to end application of thermal energy.

The treatment system **10A** and an actuation method for the treatment system **10A** have effects identical to effects of the treatment system **10** or the like. Additionally, the treatment system **10A** and the actuation method easily control the power source **83** for heat generation.

Third Embodiment

A treatment system **10B** according to a third embodiment will be described. Since the treatment system **10B** is similar to the treatment system **10** or the like, constituent elements having identical functions are denoted by identical reference numerals, and a description of the constituent elements will be omitted.

As shown in FIG. 9, in the treatment system **10B**, a TH control section **84** repeats, in TH energy application mode, a first control mode of performing control such that temperature of a heater member **53** reaches a first temperature TA and a second control mode of performing control such that the heater member **53** becomes lower than the first temperature TA, like the treatment systems **10** and **10A**.

When the temperature of the heater member **53** reaches a predetermined second temperature TD in the second control mode, the treatment system **10B** switches to the first control

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mode. For the reason, as the treatment proceeds, a time period (tD) for the second control mode decreases. That is, $tD5 < tD4 < tD3$, $tD2$ holds in FIG. 9. Note that the second temperature TD is determined under same conditions as conditions for the second temperature TB for the treatment system 10A.

The treatment system 10B controls a power source 83 for heat generation so as to end application of thermal energy by using, as a temperature change parameter based on change in the temperature of the heater member 53, a time period (ΔT_A) to arrive at the first temperature TA or a rate ($\Delta T/\Delta t$) of rise in temperature in the first control mode or a time period (ΔT_X) to arrive at a predetermined temperature TX or a rate ($\Delta T/\Delta t$) of decrease in temperature in the second control mode, like the treatment system 10. Alternatively, in the treatment system 10B, the time period (tD) for the second control mode may be used as the temperature change parameter.

The treatment system 10B and an actuation method for the treatment system 10B have effects identical to effects of the treatment system 10A or the like, and the time period (tD) for the second control mode, in which a small amount of thermal energy is applied, is short. A time period to treatment completion can thus be shortened.

Note that, in the treatment system 10A as well, output of power (TH) for heat generation may be suspended in the second control mode, like the treatment system 10B.

Fourth Embodiment

A treatment system 10C according to a fourth embodiment will be described. Since the treatment system 10C is similar to the treatment systems 10 to 10B, constituent elements having identical functions are denoted by identical reference numerals, and a description of the constituent elements will be omitted.

As shown in FIG. 10, a power supply portion 12B of the treatment system 10C has a common power source 93 which has a high-frequency power source function and a power-source-for-heat-generation function and a change-over switch 97 which switches an output destination. The power supply portion 12B further has a common sensor 95 which has the function of an HF sensor 75 and the function of a TH sensor 85.

As already described, the high-frequency power source 73 and the power source 83 for heat generation do not simultaneously output power even in the treatment systems 10 to 10B according to the embodiment. For the reason, in the treatment system 10C, the one common power source 93 functions as a high-frequency power source or a power source for heat generation under control of a control section 94.

That is, in HF application mode, HF outputted by the common power source 93 is sent to HF lines 22a and 22b via the change-over switch 97. In TH application mode, TH outputted by the common power source 93 is sent to the TH line 23 via the change-over switch 97.

Note that the common sensor 95 functions as an HF sensor or a TH sensor and that a common panel 96 functions as an HF panel or a TH panel.

The treatment system 10C and an actuation method for the treatment system 10C have the same functions as functions of the treatment systems 10 to 10B and the like and are simple in configuration.

Note that, in a treatment system in which respective heater members are disposed at jaws 36a and 36b of a treatment instrument 11, respective power sources for heat generation may be controlled on the basis of temperatures of the heater members. Alternatively, control may be performed by one

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power source for heat generation on the basis of an average temperature of the two heater members.

Fifth Embodiment

A treatment system 10D according to a fifth embodiment will be described. Since the treatment system 10D is similar to the treatment system 10 or the like, constituent elements having identical functions are denoted by identical reference numerals, and a description of the constituent elements will be omitted.

As shown in FIG. 11, in the treatment system 10D, one pair of grasping members of a treatment instrument 11D is made up of a first grasping member (a jaw 36a) which has a first heating element (a heater member 53A) and a second grasping member (a jaw 36b) which has a second heating element (a heater member 53B). The treatment system 10D further includes a change-over switch 87 for supplying power (TH) for heat generation to the heater member 53A in the first control mode and to the heater member 53B in the second control mode.

As shown in FIG. 12, when TH energy application mode proceeds, temperature of the heater member 53A rises, and temperature of the heater member 53B declines, in the first control mode (t1set). On the other hand, the temperature of the heater member 53B rises, and the temperature of the heater member 53A declines, in the second control mode (t2set).

A control section 94 ends application of thermal energy on the basis of a temperature change parameter for the heater member 53A or 53b in the second control mode, in addition to a temperature change parameter of the heater member 53A or 53b in the first control mode.

As already described, a time period (ΔT_A) for a temperature T of the heater member 53A or 53B to rise to a first temperature TA, a rate ($\Delta T/\Delta t$) of rise in temperature, or the like can be used as the temperature change parameter. Additionally, a time period for the temperature T of the heater member 53A or 53b to decrease to a predetermined temperature, a rate of decrease, or the like can be used as the temperature change parameter.

The treatment system 10D and an actuation method for the treatment system 10D have effects identical to effects of the treatment system 10 or the like. Additionally, since TH is continuously outputted from a power source for heat generation to the treatment instrument, a treatment time period is short. In addition, since a living tissue is heated from two sides, heating unevenness is unlikely to occur.

Note that a common power source 93 which has a high-frequency power source function and a power-source-for-heat-generation function can also be used in the treatment system 10D, like the treatment system 10C.

As described above, a control method, i.e., an actuation method for a treatment system includes a step of setting a treatment condition for the treatment system including one pair of grasping members which apply high-frequency power energy and thermal energy to a grasped living tissue, a high-frequency power source which outputs high-frequency power for applying the high-frequency power energy, and a power source for heat generation which outputs power for heat generation for applying the thermal energy, a step of controlling the high-frequency power source on the basis of the treatment condition and applying the high-frequency power energy to the living tissue, a step of acquiring a parameter, on the basis of change in temperature of the heating element in a first control mode of performing control such that the heating element reaches a first temperature or a second control mode

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of performing control such that the heating element becomes lower than the first temperature, during application of the thermal energy by repeating the first control mode and the second control mode on the basis of the treatment condition after application of the high-frequency power energy is ended 5 on the basis of the treatment condition, and a step of ending application of the thermal energy according to the temperature change parameter.

The present invention is not limited to the above-described embodiments and the like. Various changes, modifications, 10 and the like can be made without departing from the scope of the present invention.

What is claimed is:

1. A treatment system comprising:

a power source for heat generation which outputs power for 15 heat generation;

a high-frequency power source which outputs high-frequency power;

a grasping member having a heating element which applies the power for heat generation as thermal energy to a 20 living tissue, the grasping member further having an electric conductor which applies the high-frequency power as high-frequency power energy to the living tissue; and

a control section which repeats a first control mode of 25 performing control such that the heating element reaches a first temperature and a second control mode of performing control such that the heating element becomes lower than the first temperature, and controls the power source for heat generation according to a 30 temperature change parameter based on change in temperature of the heating element in the first control mode or the second control mode so as to end application of the thermal energy; wherein

the control section controls the high-frequency power 35 source and the power source for heat generation after application of the high-frequency power energy ends so as to start application of the thermal energy.

2. The treatment system according to claim 1, wherein the temperature change parameter comprises at least one of a 40 time period for the heating element to arrive at a predetermined temperature or a rate of change in temperature.

3. The treatment system according to claim 1, wherein the control section performs control in the second control mode such that the heating element reaches a second temperature. 45

4. The treatment system according to claim 1, wherein the treatment system switches to the first control mode when the heating element reaches a predetermined temperature in the second control mode.

5. The treatment system according to claim 4, wherein the temperature change parameter comprises a time period for the second control mode. 50

6. The treatment system according to claim 1, wherein application of the high-frequency power energy is ended when completion of a process of destroying a cell membrane in the living tissue is sensed on the basis of change in an impedance for the high-frequency power, moisture is removed from the living tissue through application of the thermal energy, and the living tissue is joined through hydrogen bonding. 60

7. The treatment system according to claim 1, wherein the high-frequency power source and the power source for heat generation are made up of a common power source.

8. The treatment system according to claim 7, wherein application of the high-frequency power energy is ended 65 when completion of a process of destroying a cell membrane in the living tissue is sensed on the basis of change in an

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impedance for the high-frequency power, moisture is removed from the living tissue through application of the thermal energy, and the living tissue is joined through hydrogen bonding.

9. An actuation method for a treatment system, comprising:

a step of setting a treatment condition for the treatment system including a grasping member having a heating element which applies thermal energy to a living tissue and a power source for heat generation which outputs power for heat generation for applying the thermal energy;

a step of acquiring a temperature change parameter, on the basis of change in temperature of the heating element in a first control mode of performing control such that the heating element reaches a first temperature or a second control mode of performing control such that the heating element becomes lower than the first temperature, during application of the thermal energy by repeating the first control mode and the second control mode on the basis of the treatment condition; and

a step of ending application of the thermal energy according to the temperature change parameter; wherein the grasping member further having an electrode which applies high-frequency power outputted by a high-frequency power source as high-frequency power energy to the living tissue, and

the actuation method further comprises a step of applying the high-frequency power energy to the living tissue before application of the thermal energy.

10. The actuation method for the treatment system according to claim 9, wherein the temperature change parameter comprises at least one of a time period for the heating element to arrive at a predetermined temperature or a rate of change in temperature of the heating element.

11. The actuation method for the treatment system according to claim 9, wherein the control section performs control in the second control mode such that the heating element reaches a second temperature.

12. The actuation method for the treatment system according to claim 9, wherein the treatment system switches to the first control mode when the heating element reaches a predetermined temperature in the second control mode.

13. The actuation method for the treatment system according to claim 12, wherein the temperature change parameter comprises a time period for the second control mode.

14. The actuation method for the treatment system according to claim 9, wherein application of high-frequency power energy is ended when completion of a process of destroying a cell membrane in the living tissue is sensed on the basis of change in an impedance for the high-frequency power, moisture is removed from the living tissue through application of the thermal energy, and the living tissue is joined through hydrogen bonding.

15. The actuation method for the treatment system according to claim 9, wherein the high-frequency power source and the power source for heat generation are made up of a common power source.

16. A treatment system comprising:

a high-frequency power source which outputs high-frequency power;

a power source for heat generation which outputs power for heat generation;

one pair of grasping members adapted to grasp a living tissue, the grasping members having an electric conductor which applies the high-frequency power as high-frequency power energy and is disposed at each of the two grasping members and a heating element which

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applies the power for heat generation as thermal energy to the living tissue, is disposed at least one of the grasping members, and is made of a material having a positive temperature coefficient of resistance; and
a control section which controls the high-frequency power source and the power source for heat generation after application of the high-frequency power energy ends so as to start application of the thermal energy, and repeats a first control mode of performing control such that the heating element reaches a first temperature and a second control mode of performing control such that the heating element becomes lower than the first temperature, and controls the power source for heat generation according to a temperature change parameter based on change in temperature of the heating element in the first control mode or the second control mode so as to end application of the thermal energy, after application of the thermal energy starts.

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